# Low-dose-rate X-ray detection using a direct-conversion ceramic-substrate silicon diode and a 5.0 m coaxial cable

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(Accepted October 6, 2014)

# Abstract

A direct-conversion silicon X-ray diode (Si-XD) is very useful for detecting low-dose-rate X-rays. The Si-XD is a selected high-sensitivity Si photodiode for detecting X-rays. In this experiment, the Si-XD is connected to an X-ray detecting module through a 5.0 m coaxial cable. The photocurrents flowing through the Si-XD are converted into voltages and amplified using current-voltage (I-V) and voltage-voltage (V-V) amplifiers in the module. At a constant tube current of 0.8 mA, the output voltage increased with increasing tube voltage. The output voltage was proportional to the tube current at a tube voltage of 80 kV.

Keywords: Si X-ray diode, direct conversion, ceramic substrate, X-ray detecting module, CT detector

# 1. Introduction

To perform molecular imaging using X-rays, we developed several photon-counting energydispersive X-ray computed tomography (ED-CT) systems.<sup>1-4)</sup> In the ED-CT systems, we usually used cadmium telluride (CdTe) detectors with an energy resolution of 1 % at 122 keV to disperse photon energy. Subsequently, 2-keV-width iodine K-edge CT was performed using s silicon PIN diode,<sup>5)</sup> and blood vessels were observed at high contrast.

Recently, we have found a high-sensitivity silicon X-ray diode (Si-XD)<sup>6.7)</sup> with a ceramic substrate, and a high-sensitivity CT system has been developed using a direct-conversion Si-XD without scintillators. In addition, gadolinium K-edge imaging has also been carried out utilizing an ED-CT system with the Si-XD by determining threshold photon energy.

Using the Si-XD in conjunction with an X-ray detecting module, although low-dose-rate X-rays can

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Fig. 1. Block diagram for detecting low-dose-rate X-rays using a Si-XD, a 5.0-m coaxial cable, an X-ray detecting module, and an X-ray generator. The Si-XD is placed 1.0 m from the X-ray source, and the output voltage is measured using a digital voltage meter with an integrator.



Fig. 2. Experimental setup for detecting X-rays.

be detected, we have to use a long coaxial cable between the Si-XD and the module to construct a new module consisting of an analog digital converter (ADC) and amplifiers. Therefore, we have to measure the output voltage when a Si-XD is connected to the module using the long cable. Therefore, we constructed an experimental setup using the long cable and measured X-ray sensitivity of the Si-XD.

# 2. Experimental methods

#### 2.1. Low-dose-rate X-ray detection

Figure 1 shows a block diagram for detecting low-dose-rate X-rays using a Si-XD (S1087-01, Hamamatsu). Using the Si-XD detector, X-ray photons are detected directly by the light receiving



Fig. 3. Circuit diagrams of I-V and V-V amplifiers in the X-ray detecting module.

surface of  $1.3 \times 1.3 \text{ mm}^2$ , and the detector is shielded using an aluminum (Al) case with a  $25-\mu$ m-thick Al window and a BNC connector. Subsequently, the detector is connected to an X-ray detecting module through a 5.0-m-length coaxial cable (Fig. 2), and the output is measured using a digital voltage meter and a 4.7-s-time-constant integrator for voltage smoothing.

#### 2.2. X-ray detecting module

In the module, the photocurrents flowing through the Si-PIN are converted into voltages and amplified using current-voltage (I-V) and voltage-voltage (V-V) amplifiers, and the output from a small connector (ERA.00.250.CTL, Lemo) is measured using a digital voltage meter. To construct low-noise high-sensitivity amplifiers, a low-ripple smoothing circuit for an alternating current (AC) adopter is necessary.

The main circuit diagrams of the X-ray detecting module are shown in Fig. 3. The photocurrents are converted into voltages using the inverse I-V amplifier with a 2-fA-bias 2-channel operational amplifier (LMC662, National Semiconductor). The V-V amplifier utilizes the second channel of LMC662 with a non-inverse amplifying circuit. The gain of the V-V amplifier increases with increasing resistance in a  $50 \text{ k}\Omega$  variable resistor.



Fig. 4. X-ray dose rate measured using an ionization chamber placed 1.0 m from the X-ray source. (a) Tube voltage dependence at a tube current of 0.8 mA, and (b) tube current dependence at a tube voltage of 80 kV.

# 3. Results

#### 3.1. X-ray dose rate

The measurement of X-ray dose rate is very important because the relative sensitivities of the detectors are roughly proportional to the dose rate. The X-ray dose rate from the X-ray generator was measured using an ionization chamber (RAMTEC 1000 plus, Toyo Medic) without filtration (Fig. 4). The chamber was placed 1.0 m from the X-ray source. At a constant tube current of 0.8 mA, the X-ray dose rate increased with increasing tube voltage [Fig. 4(a)]. On the other hand, the dose rate was proportional to the tube current at a constant tube voltage of 80 kV [Fig. 4(b)]. At a tube voltage of 80 kV and a current of 0.8 mA, the X-ray dose rate was  $53.7 \,\mu$ Gy/s.



Fig. 5. Output voltages from the module. (a) Variations with the tube voltage at a tube current of 0.8 mA, and (b) variations with the tube current at a tube voltage of 80 kV.

#### 3.2. Module output

Figure 5 shows the output voltages from the Si-XD detector measured using the X-ray detecting module. At a tube current of 0.8 mA, the output increased with increasing tube voltage [Fig. 5(a)]. As shown in Fig. 5(b), the output voltage was in proportion to the tube current at a tube voltage of 80 kV.

# 4. Discussion and conclusions

We constructed a low-dose-rate low-noise X-ray detecting module for semiconductor diodes, and this module with an ADC and a tablet personal computer will be applied soon to a compact X-ray dosimeter. In particular, the Si-XD was connected to the X-ray detecting module using a 5.0-m-length coaxial cable, since we had to measure output voltages using the cable.

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In the former experiment, the Si-XD was connected directly to the module. In the near future, the X-ray detecting module consisting of an ADC and the two amplifiers would be developed to measure X-ray dose to avoid radiation exposure for observers.

# Acknowledgments

This work was supported by Grants from Keiryo Research Foundation, Promotion and Mutual Aid Corporation for Private Schools of Japan, Japan Science and Technology Agency (JST), and Ministry of Education, Culture, Sports, Science and Technology of Japan (MEXT). This was also supported by a Grant-in-Aid for Strategic Medical Science Research Center from MEXT, 2009-2013 and 2014-2018.

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